1	Preparation and Characterization of Dissolving Ulvan Microneedle for
2	Transdermal Delivery System
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6	Outline
7	1. Introduction
8	2. Ulvan extraction and chemical analysis
9	3. Microneedle fabrication and characterization
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14	Abstract
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16	Transdermal drug delivery system (TDDS) is a noninvasive method of delivering drugs across
17	the skin. However, TDDS is limited by stratum corneum barrier, thus only small (MW $< 500$
18	Da) and hydrophobic molecules can be delivered. Microneedle (MN) can enhance the
19 20	efficiency of TDDS via minimally invasive and pain-free method. Recently, a dissolving MN
20	made of natural polymers has gain many attentions due to its rapid dissolving ability and good
21	biocompatibility. In this study, we are the first group to fabricate and characterize a dissolving
22	MN made from ulvan (UMN), a sulfated polysaccharide extracted from <i>Ulva lactuca</i> . The
23	UMNs were fabricated through an easy and mild two-step casting method. The MN had two
24 25	layers, the needle layer is made from ulvan and loaded with ascorbic acid 2-glucoside (AA2G), and the healting layer is made from a mixture of polyginylayrrelidene (DVD) and
	and the backing layer is made from a mixture of polyvinylpyrrolidone (PVP) and
26 27	carboxymethyl cellulose (CMC). The UMN has pyramidal-shaped needles, 652-682 μm in height, 248-280 μm in base width and 2.47-2.75 in aspect ratio. 4% UMN had the nearest aspect
27	ratio to the master mold and used as the base material of the needle layer. The <i>in vitro</i> skin
28 29	insertion study showed the MN successfully penetrated the porcine skin and Parafilm layers.
30	The incorporation of 2.0% AA2G into the MN can increase the insertion ratio and depth of
31	UMN. The <i>in vitro</i> dissolution studies showed that UMN completely dissolved after inserted
32	for approximately 2 min. The confocal laser scanning microscopic images showed that the drug
33	can diffuse into the depth of 300-500 $\mu$ m, which is similar to the depth of skin dermis layer.
34	The <i>in vitro</i> drug permeation profiles revealed different release behavior of AA2G-loaded
35	UMN, 0.5% AA2G-loaded UMN showed a burst release in the first 30 min, while 1.0% and
36	2.0% AA2G-loaded UMN showed a sustained release. The cumulative release amount of
37	AA2G after 3 h was about 80-90%, which was higher than the solution group (40%). Briefly,
38	this study demonstrated that UMN can enhance the transdermal delivery efficiency of AA2G

39 and have the potential to be used in pharmaceutical or cosmeceutical fields.

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